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Abstract:	<p>The purpose of this in vitro study was to compare the primary stability and removal torque of bone level and tissue level implants in different bone quality. Fifteen tissue level and bone level implants (3.3x10mm and 4.1x10mm) were used for assessing the stability in type II and type IV bone. Forty bovine rib blocks were used in this study. The primary stability of the implant was measured by the resonance frequency using an Osstel® device. The removal torque values (RTV) of the implants was assessed using a Digital torque gauge instrument. The Implant Stability Quotient (ISQ) values and the RTV showed a marginally higher stability with bone level implants as compared to tissue level implants. However, these differences were not statistically significant in both type of bone used ($P>0.05$). On the other hand, compared to type IV, type II bone showed significant differences in the ISQ ($P<0.01$) and RTV ($P<0.001$) of bone level and tissue level implants. The study concluded that bone quality is an important factor in establishing primary stability than the implant dimension. Bone level and tissue level implants of same dimensions can be selected based on the esthetic demands since they showed similar mechanical properties.</p>

1 **Impact of one quality and implant type on the primary stability: an experimental study**
2 **using bovine bone.**

3
4 **Abstract**

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6 of bone level and tissue level implants in different bone quality. Fifteen tissue level and
7 bone level implants (3.3x10mm and 4.1x10mm) were used for assessing the stability in type
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18 on the esthetic demands since they showed similar mechanical properties.

19
20 **Key Words:** *implants; removal torque; primary stability; osseointegration; resonance*
21 *frequency analysis.*

22

23 **Introduction**

24 Successful osseointegration has an important influence on the long term success of dental
25 implant restorations. While primary implant stability and osseointegration can be
26 predictably achieved in dense bone, it is often challenging to achieve the same in areas with
27 poor bone quality.¹ Primary stability lowers the level of implant micromotion, which in turn
28 allows uninhibited healing and osseointegration.² Friberg et al³ reported an implant failure
29 rate of 32% for those implants that showed inadequate initial stability.

30
31 Studies have demonstrated that initial implant stability is influenced by factors such as the
32 length and diameter of the implant, the implant design, the micro-morphology of the
33 implant surface, the insertion technique, and the congruity between the implant and the
34 surrounding bone.⁴⁻⁷ Further important determinants are the quality and quantity of the
35 bone. Low density bone implant sites have been pointed out as the greatest potential risk
36 factor for implant loss when working with standard bone drilling protocols.^{8,9} Clinical study
37 with consecutively placed implants that were immediately loaded showed a higher failure
38 rate in low density bone, reinforcing that primary stability is a major determinant in the
39 success of immediately loaded implants.^{10,11}

40
41 The success of implant depends on the bone quality and the healing at the at the implant-
42 bone interface. The structural and material properties of bone such as mineral density and
43 mineral maturity are important contributors to bone strength^{12,13}. Even though majority of
44 literature defines the bone quality in terms of bone density, other biological factors such as
45 bone metabolism, cell turnover, mineralization, maturation, intercellular matrix, and
46 vascularity are also factors that influence the osseointegration.^{11,12} The stiffness of the bone
47 around the implant increases during the process of osseointegration, and the interlocks
48 between bones and implant surface prevents micro-motion and formation of fibrous scar
49 tissue when the implant is loaded properly.^{14,15} Basically, the stability of implantation is
50 largely associated with osseointegration and peri-implant bone remodeling during healing
51 process .

52
53 Bone level implants were introduced by the International Team for Implantology (ITI) to
54 minimize crestal bone loss and to improve the esthetic predictability of implant-based

55 restorations. The biomechanical properties of these implants are not thoroughly explored.
56 Also the claim that these implants have lesser crestal bone loss compared to tissue level
57 implants is also controversial. The reason for this controversy is that implant abutment
58 junction (microgap) is closer to the bone which may results in more bone loss. However, in
59 terms of esthetic point of view bone level implants are superior to tissue level implants.¹⁶
60
61 Number methods are used to assess the primary stability of the dental implant.¹⁷ Among
62 these resonance frequency analysis has been revealed and widely used as the most
63 successful method to assess primary stability because of its easiness, accuracy, and non-
64 invasiveness.^{1, 18} The implant-bone interface is measured based by resonance frequency (RF)
65 which is the reaction to oscillations exerted to the implant, and is expressed as implant
66 stability quotient (ISQ).¹⁹ On the other hand mechanical test such as insertion torque and
67 values of push-out test showed positive correlation to the primary stability.^{20, 21} Hence
68 noninvasive measurement methods have also been introduced for the diagnosis and
69 prediction of immediate and the long-term implant stability. Studies have shown that the
70 measurement of removal torque strength was a useful indirect biomechanical method to
71 evaluate the bone and implant interface.^{22, 23} The purpose of this in vitro study was to
72 compare the primary stability and removal torque measurements of bone level and tissue
73 level implants in different bone quality.

74

75 **Materials and methods**

76 Fresh bovine ribs procured from the butcher shop were used for the study. They were cut
77 into 6 cm long pieces and a total of 40 bovine rib blocks were prepared. The cortical bone
78 was removed until it was about 1 mm thick in order to make it mimic to type II bone.²⁴ The
79 other 20 blocks had all cortical bone removed and exposed the trabecular bone to make it
80 similar to type IV bone (Fig 1). 20 tissue level (standard plus) and 20 bone level implants
81 with two different dimensions (3.3 x10 and 4.1x10) were installed in each rib blocks (Fig 2).

82

83 **Resonance frequency (RF)**

84 After installation, the ISQ was measured by using resonance frequency analyzer (Osstell,
85 Osstell AB, Goteborg, Sweden). The osteotomy sites were prepared according to the
86 manufacturer's guidelines. After implant insertion, the magnetic wireless RF analyzer was
87 used for direct measurement of the endosseous implant stability. The RF analysis technique

88 analyzes the RF range (110–10000 Hz) of a smartpeg® which can be attached to the implant.
89 The probe of wireless RF analyzer, Osstell Mentor™ was held perpendicular to the implant
90 as indicated by the manufacturer (Fig 3).

91

92 **Removal torque values (RTV)**

93 The RTV of each implant was measured using a digital torque MGT 50® digital torque gauge
94 instrument (MARK-10 Corp., New York). A controlled, gradually increasing rotational force
95 (displacement 0.5 mm min⁻¹) was applied to the implant until implant loosening (Fig 4). The
96 peak force measured at implant loosening was scored as the torque-out value.²⁵

97

98 **Statistical Analysis**

99 The statistical analysis was performed with GraphPad® InStat 3.05 software (GraphPad
100 Software Inc, San Diego, CA, USA) using analysis of variance (ANOVA). Tukey-Kramer
101 multiple comparisons test was used to compare the ISQ values and RTV of the two types of
102 implants with two different dimensions. p-values <0.05 were assumed to be statistically
103 significant.

104

105 **Results**

106 The mean values and standard deviations of resonance frequency measurements are shown
107 in Figure 5. Bone level implants showed ISQ values of 67.35 ± 5.21 and 71.65 ± 5.85
108 respectively for the 3.3 and 4.1 diameter implants. These values were higher than tissue
109 level implants of the same dimension. Similar results were also found in type IV bone (Fig
110 5). Compared to type IV bone, the primary stability of type II bone showed significantly
111 higher values ($P < 0.01$) for the 3.3 and 4.1 diameter implants.

112

113 The removal torque values are depicted in Figure 6. The removal torque measurements
114 showed no significant differences between bone level and tissue level implants with the two
115 different dimensions of the implants used (Fig 6). However, significantly lower removal
116 torque values were observed in type IV bone as compared to the type II bone ($P < 0.001$).

117

118

119 **Discussion**

120 Implant stability is a prerequisite for the long-term clinical success of osseointegrated
121 implants.^{26, 27} The stability of implants can be successfully assessed by the Osstell device

122 which quantifies the RF. Resonance frequency is a noninvasive, objective method to
123 evaluate implant stability and it has been validated through *in vitro* and *in vivo* studies.^{19, 28}
124 The technique is based on the measurement of the RF of a small piezoelectric transducer
125 attached to an implant or abutment.^{19, 29}

126
127 It is well known that primary stability of implants depends on surgical techniques used, bone
128 density, and implant design.³⁰⁻³² Maintenance of low implant micro-movement, especially in
129 the early healing phase is important to promote direct bone in growth to implant surface.³³
130 Earlier studies have shown a linear relationship between the exposed implant height and
131 the corresponding ISQ values.^{21, 34} Sim and Lang³⁵ reported a correlation between the ISQ
132 values and the bone structure and implant length. On the other hand O'Sullivan et al³⁶
133 failed to report any correlation between the implant primary stability and the shape of the
134 implant. In the present study a comparison was done between bone level implants and
135 tissue level implants with similar dimensions. Bone level implants showed slightly higher but
136 insignificant ISQ and removal torque values as compared to the tissue level implants.

137
138 However, when the primary stability implants were compared in different bone quality, a
139 statistically higher ISQ values were observed for implants inserted in Type II bone with 1 mm
140 cortical bone. This observation is in agreement with observation of Akca et al³⁷ who
141 reported that bone quality had more influence than implant shape. Elias et al¹⁵ concluded
142 that implant design, surgical technique and substrate type are the major components
143 influencing the primary stability.

144
145 Bovine rib was used in this study and is classified as type II bone in other studies since
146 contains thick compact bone and dense trabecular bone.³⁸ In order to mimic the type IV
147 bone the entire cortical bone is removed. The lower ISQ values and removal torque
148 observed in this experiment indicates that the bone quality is an important determinant in
149 the early implant stability. There were significant correlations between bone density and
150 removal torque values which is in agreement with earlier studies.^{39, 40}

151

152 To evaluate the initial bone quality and degree of osseointegration, various methods have
153 been proposed ⁴¹, including histology and histomorphometry ⁴²⁻⁴⁵, removal torque
154 analysis, ⁴⁶⁻⁴⁸ pull- and push-through tests ⁴⁹ and X-ray examination ³⁰. RFA has been used to
155 study the factors, including surgical technique, loading protocol, and implant design that
156 govern implant stability. The implant stability can also vary with a change in osseous
157 remodeling and percentage of implant bone interface contact. ⁵⁰ The major drawback of the
158 RFA analysis is that it can only reflect the mechanical property of the bone-implant
159 interfacial layer by assessing the changes of stiffness during osseointegration process. ^{29, 41,}
160 ⁵¹ Even though it is an excellent nondestructive method its clinical application is limited to
161 establish the implant stability and the prognostic criteria for long-term implant success. ^{52, 53}

162

163 Within the limitations of the study, it can be assumed that bone quality is an important
164 factor in establishing primary stability than the implant dimension from the biomechanical
165 point. The main limitation of the present study is that the mechanical characteristics of the
166 primary stability of an implant were considered in an *in vitro setup* using bovine bone.
167 Further *in vivo* studies are required to understand the actual clinical situation in which many
168 biological factors influence the primary stability of implants. Moreover secondary stability
169 tests, finite element studies (FEA) and histomorphometric studies are necessary to
170 substantiate the present observations. ⁵⁴ The priority for selecting either a bone level or a
171 tissue level implant of same dimension should be based on the esthetic demands since they
172 showed similar mechanical properties.

173

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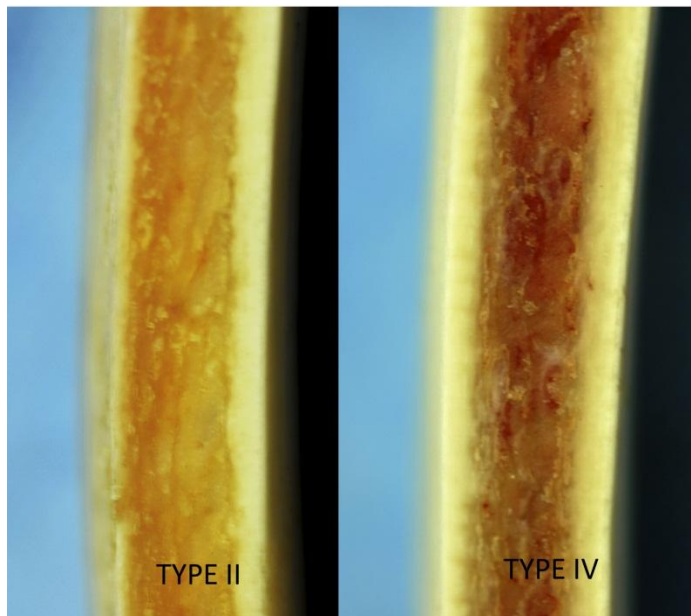
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372 **Legends to figures**

373 Figure - 1. The bovine rib showing type II and type IV bone .



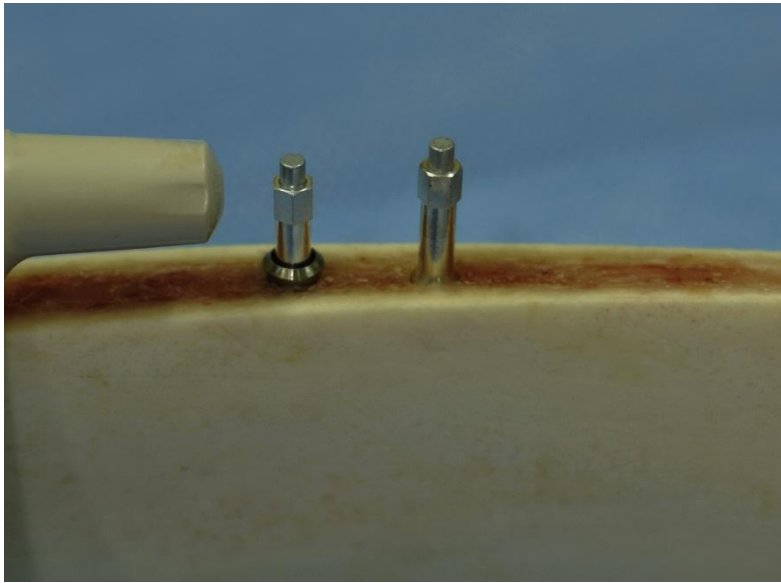
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375 Figure - 2. Illustration showing the positioning of tissue level and bone level implants.



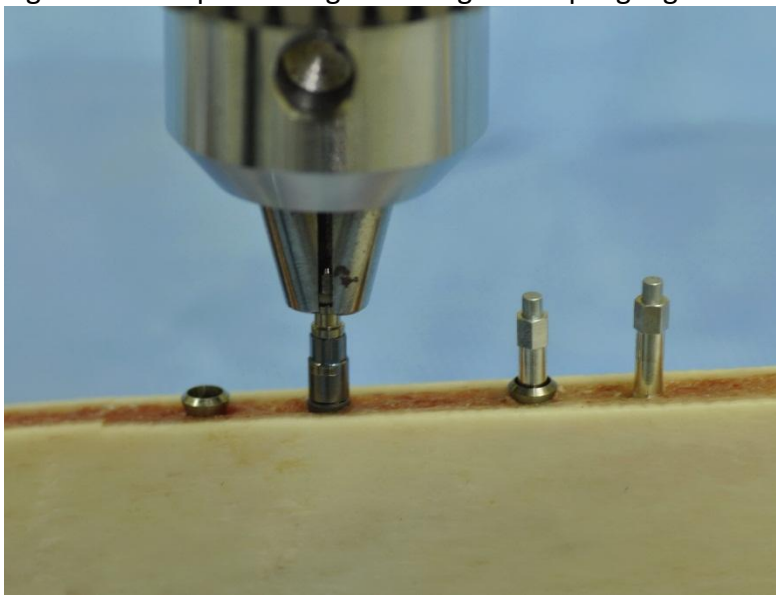
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377 Figure - 3. The implant in position with the SmartPeg™ and the tip of the Ostell Mentor
378 resonance frequency analyser.



379

380 Figure - 4. The positioning of the digital torque gauge.

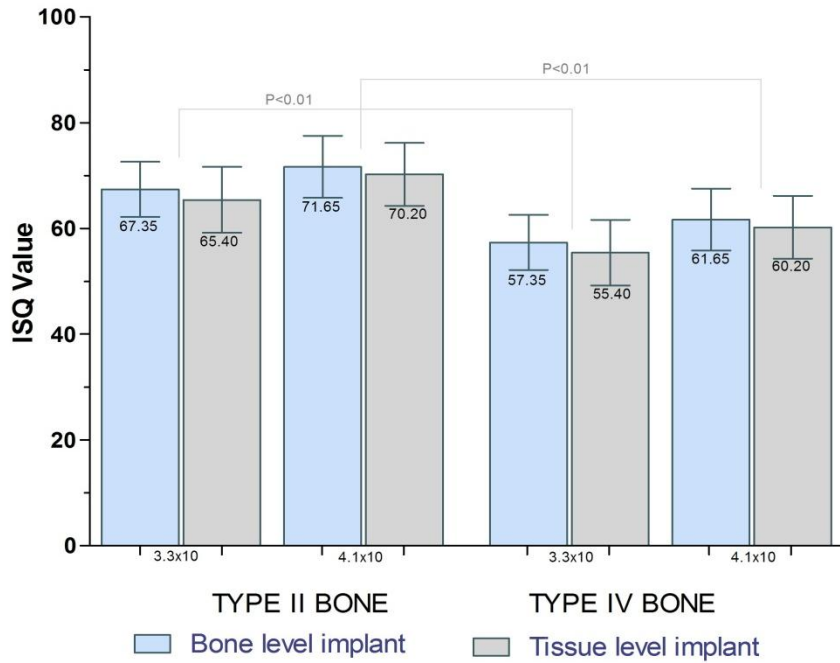


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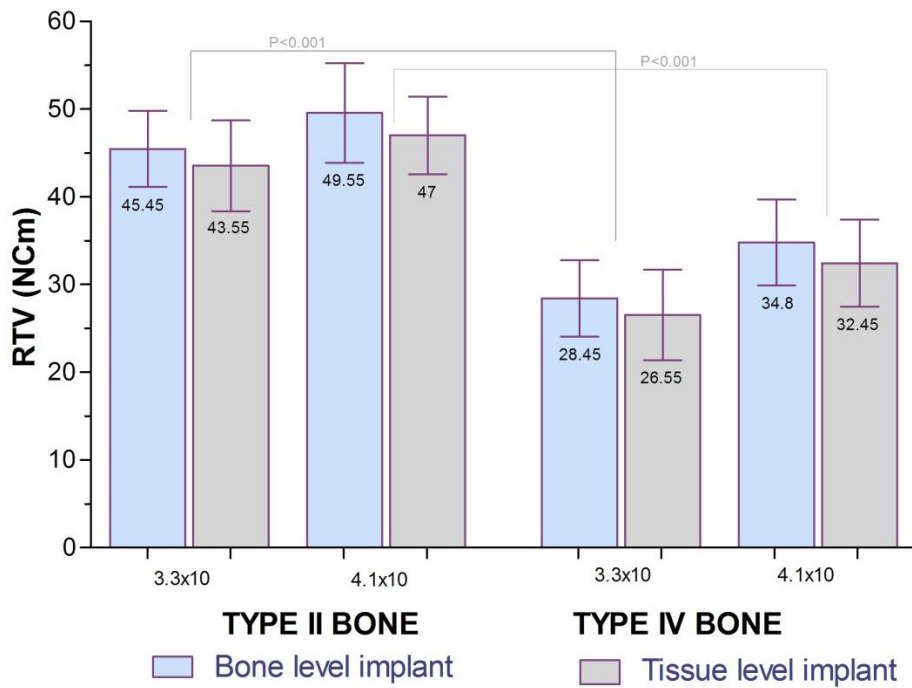
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384 Figure-5. The RF values (ISQ) of bone level and tissue level implants in Type II and type IV
 385 bone.



386

387 Figure-6. The removal torque values (RTV) of bone level and tissue level implants in Type II
 388 and type IV bone.



389